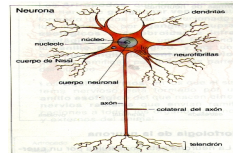
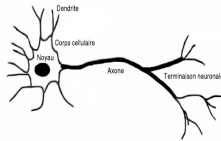
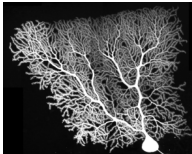


# Integrate and Fire models for neural networks and spontaneous activity

Benoît Perthame



The electrically active cells are described by an **action potential**

■ Hodgkin-Huxley

■ FitzHugh-Nagumo

■ Morris-Lekar

■ Mitchell-Schaeffer

$$C \frac{dv}{dt} = I - g_{Na} m^3 h (V - V_{Na}) - g_K n^4 (V - V_K) - g_L (V - V_L)$$

$$\frac{dm}{dt} = a_m(V)(1-m) - b_m(V)m$$

$$\frac{dh}{dt} = a_h(V)(1-h) - b_h(V)h$$

$$\frac{dn}{dt} = a_n(V)(1-n) - b_n(V)n$$

$$a_m(V) = .1(V + 40)/(1 - \exp(-(V + 40)/10))$$

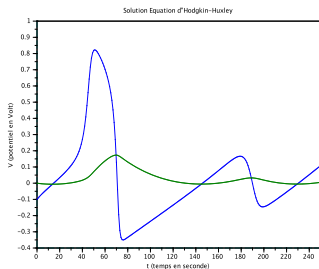
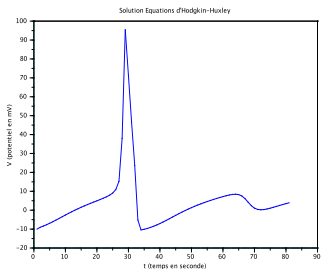
$$b_m(V) = 4 \exp(-(V + 65)/18)$$

$$a_h(V) = .07 \exp(-(V + 65)/20)$$

$$b_h(V) = 1/(1 + \exp(-(V + 35)/10))$$

$$a_n(V) = .01(V + 55)/(1 - \exp(-(V + 55)/10))$$

$$b_n(V) = .125 \exp(-(V + 65)/80)$$



## Solutions of Hodgkin-Huxley's model and of FitzHugh-Nagumo's model

- These models are accurate
- but very expensive/difficult to use for large assemblies of neurones.

The **Wilson-Cowan** model (1972) describes the firing rates  $N(x, t)$  of neuron assemblies located at position  $x$  through an integral equation

$$\frac{d}{dt}N(x, t) = -N(x, t) + \int w(x, y)\sigma(N(y, t))dy + s(x, t)$$

- $\sigma(\cdot)$  = sigmoid
- $w(x, y)$  = connectivity matrix
- $s$  = source

Can be seen as a generic model of network.  
Not physiologically based

Feature : multiple steady states and bifurcation theory  
(Bressloff-Golubitsky, Chossat-Faugeras-Faye)

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**Feature** : multiple steady states and bifurcation theory  
(Bressloff-Golubitsky, Chossat-Faugeras-Faye)

**Aim** : large scale brain activity, visual hallucinations (Klüver, Oster, Siegel...)



**Generic goal** : understand physiologically based models of neural networks.

- I. Principle of Noisy Integrate and Fire model
- II. The nonlinear Noisy Integrate and Fire model
- III. The voltage-conductance kinetic system for integrate&fire
- IV. The elapsed time approach



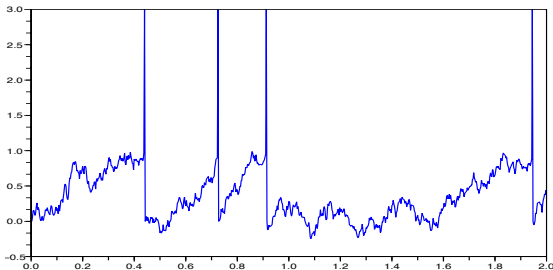
The Leaky Integrate & Fire model is simpler

$$dV(t) = (-V(t) + I(t))dt + \sigma dW(t), \quad V(t) < V_{\text{Firing}}$$

$$V(t_-) = V_{\text{Firing}} \implies V(t_+) = V_{\text{reset}}$$

The idea was introduced by **L. Lapicque (1907)**

- $I(t)$  input current
- Noise or not
- Stochastic firing
- Much simpler than Hodgkin-Huxley/FitzHugh-Nagumo models



Solution to the LIF model

- N. Brunel and V. Hakim, R. Brette, W. Gerstner and W. Kistler, Omurtag, Knight and Sirovich, Cai and Tao...
- Fit to measurements
- Explains quantitatively observations on the brain activity



**FIGURE 4 | Fitting spiking models to electrophysiological recordings. (A)** The response of a cortical pyramidal cell to a fluctuating current (from the INCF competition) is fitted to various models: MAT (Kobayashi et al., 2003), adaptive integrate-and-fire, and Izhikovich (2003). Performance on the training data is indicated on the right as the gamma factor (close to the proportion of predicted spikes), relative to the intrinsic gamma factor of the neuron (i.e., proportion of common spikes between two trials). Note that the voltage units for the models are irrelevant (only spike trains are fitted). **(B)** The response of an anteroventral cochlear nucleus (brain slice made from a P12 mouse, see Methods in Magnusson et al., 2008) to the same fluctuating current is fitted to an adaptive exponential integrate-and-fire [Brette and Gerstner, 2005; note that the responses do not correspond to the same portion of the current as in **(A)**]. The cell was electrophysiologically characterized as a stellate cell (Fujino and Oertel, 2001). The performance was  $\Gamma = 0.39$  in this case (trial-to-trial variability was not available for this recording).

From C. Rossant et al, *Frontiers in Neuroscience* (2011)

## Open question :

Derive rigorously the Integrate and Fire model from the FHN system.

The probability  $n(v, t)$  to find a neuron at the potential  $v$  solves the Fokker-Planck Eq. for  $v \leq V_F$

$$\left\{ \begin{array}{l} \frac{\partial n(v, t)}{\partial t} + \frac{\partial}{\partial v} \left[ \overbrace{(-v + I(t)) n(v, t)}^{\text{leak+external currents}} \right] - \overbrace{a \frac{\partial^2 n(v, t)}{\partial v^2}}^{\text{Noise}} = \overbrace{N(t) \delta(v = V_R)}^{\text{neurons reset}}, \\ n(V_F, t) = 0, \quad n(-\infty, t) = 0, \\ N(t) := -a \frac{\partial n(V_F, t)}{\partial v} \geq 0, \quad (\text{the total flux of neurons firing at } V_F). \end{array} \right.$$

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$N(t)$  is also a Lagrange multiplier for the constraint

$$\int_{-\infty}^{V_F} n(v, t) dv = 1.$$

$$\left\{ \begin{array}{l} \frac{\partial n(v,t)}{\partial t} + \frac{\partial}{\partial v} [(-v + I(t))n(v,t)] - a \frac{\partial^2 n(v,t)}{\partial v^2} = N(t) \delta(v - V_R), \quad v \\ n(V_F, t) = 0, \quad n(-\infty, t) = 0 \\ N(t) := -a \frac{\partial n(V_F, t)}{\partial v} \geq 0, \quad (\text{the total flux of firing neurons at } V_F). \end{array} \right.$$

**Properties (Cáceres, Carrillo, BP)** For  $I(t) \equiv 0$  the solutions satisfy

- $n \geq 0$ ,  $\int_{-\infty}^{V_F} n(v, t) dv = 1$ ,
- $n(v, t) \xrightarrow{t \rightarrow \infty} P(v)$  the unique steady state (probability density)
- The convergence rate is exponential

**Conclusion** Total desynchronization

The proof uses

- the Relative Entropy. For  $H(\cdot)$  convex,

$$\frac{d}{dt} \int_{-\infty}^{V_F} P(v) H\left(\frac{n(v, t)}{P(v)}\right) dv \leq 0,$$

- Hardy/Poincaré inequality,

$$\int_{-\infty}^{V_F} P(v) |u(v)|^2 dv \leq C \int_{-\infty}^{V_F} P(v) |\nabla u(v)|^2 dv,$$

when 
$$\int_{-\infty}^{V_F} P(v) u(v) dv = 0, \quad P(V_F) = 0$$

See : Ledoux, Barthe and Roberto



For networks, the current  $I(t) = bN(t)$  is related to the network activity

$$\left\{ \begin{array}{l} \frac{\partial n(v,t)}{\partial t} + \frac{\partial}{\partial v} [(-v + bN(t))n(v,t)] - a(N(t)) \frac{\partial^2 n(v,t)}{\partial v^2} = N(t) \delta_{V_R}(v), \\ n(V_F, t) = 0, \quad n(-\infty, t) = 0, \\ N(t) := -a(N(t)) \frac{\partial}{\partial v} n(V_F, t) \geq 0, \quad \text{total flux of firing neurons at } V_F \end{array} \right.$$

## Constitutive laws

■  $b =$  connectivity

■  $b > 0$  for excitatory neurones  
neurones

■  $b < 0$  for inhibitory

■  $a(N) = a_0 + a_1 N$

$$\left\{ \begin{array}{l} \frac{\partial n(v,t)}{\partial t} + \frac{\partial}{\partial v} [(-v + bN(t))n(v,t)] - a(N(t)) \frac{\partial^2 n(v,t)}{\partial v^2} = N(t) \delta_{V_R}(v), \\ n(V_F, t) = 0, \quad n(-\infty, t) = 0, \\ N(t) := -a(N(t)) \frac{\partial}{\partial v} n(V_F, t) \geq 0, \quad \text{total flux of firing neurons at } V_F \end{array} \right.$$

Can be derived from a large system of  $N$  interacting neurons, see  
 Delarue, Inglis, Rubenthaler, Tanre : for  $1 \leq i \leq N$

$$\frac{d}{dt} V_i(t) = -V_i(t) + \frac{\beta}{N} \sum_{j=1}^N \sum_{\tau_j} \delta(t - \tau_j) + \sigma dW_i(t), \quad V_i(t) < V_F,$$

with  $\tau_j$  the spiking times  $V_j(\tau_j) = V_F$ .

## Theorem (J. Carrillo, D. Salort, BP, D. Smets)[inhibitory]

Assume

- $a = a_0 > 0$  and  $b < 0$  (inhibitory)
- the initial data is bounded by a supersolution (in a certain sense)

Then,

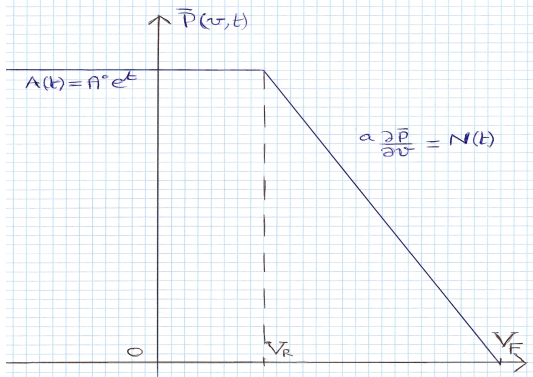
- There are global solutions
- Uniformly bounded for all  $t > 0$

**Open question** Large time convergence to the unique steady state

See also Carrillo, Gonzalés, Gualdani, Schoenbeck for a reduction to Stefan problem

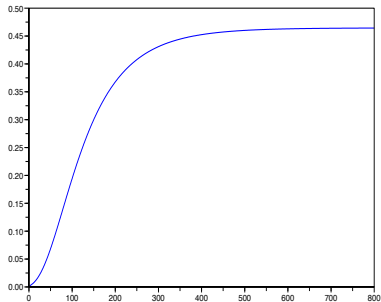
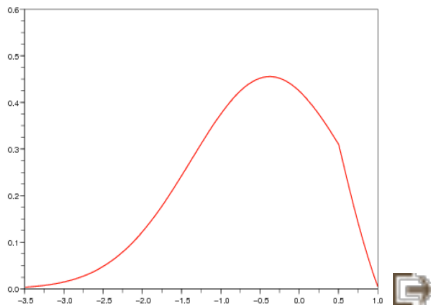
**Proof** Two ingredients :

1. A universal supersolution (whatever is  $N(t)$ )



2. For the Fokker-Planck equation, regularizing effects  $L^1 \rightarrow L^\infty$

$$\begin{cases} \frac{\partial n(v,t)}{\partial t} + \frac{\partial}{\partial v} [(-v + bN(t))n(v,t)] - a(N(t)) \frac{\partial^2 n(v,t)}{\partial v^2} = N(t) \delta_{V_R}(v), \\ n(V_F, t) = 0, \quad n(-\infty, t) = 0, \quad N(t) := -a(N(t)) \frac{\partial}{\partial v} n(V_F, t) \geq 0 \end{cases}$$



Inhibitory case  $b < 0$ . Left  $p(v, t)$ , Right :  $N(t)$

## Theorem (M. Caceres, J. Carrillo, BP) [excitatory, blow-up]

Assume  $a \geq a_0 > 0$  and  $b > 0$ . Then the solution blows-up in finite time in the two cases

- the initial data is concentrated enough around  $v = V_F$  (depending on  $b$ )
- initial data is given,  $b$  is large enough

## Surprisingly

- Noise does not help
- value of  $b$  does not count

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## Possible interpretation

- $N(t) \rightarrow \rho \delta(t - t_{BU})$  and  $t_{BU} > 0$ ,
- partial synchronization (S. Ha, Dumont-Henry, Giacomin, Pakdaman)

- Noise does not help

**Theorem (J. Carrillo, D. Salort, BP, D. Smets)[inhibitory]**

Assume  $a = a_0 + a_1 N$  and  $b < 0$ .

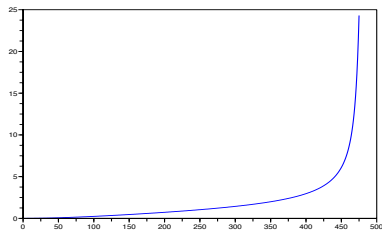
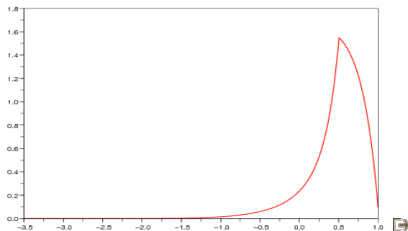
Then the solution blows-up in finite time when the initial data is concentrated enough around  $v = V_F$



**Theorem (J. Carrillo, D. Salort, BP, D. Smets) [excitatory, existence]**

Assume  $a \geq a_0 > 0$  and  $b > 0$ . Being given the initial data

- for  $b$  small enough, there is a solution
- it converges to the steady state



Excitatory integrate and fire model. Blow-up case. Left  $\rho(v, t)$ , Right :  $N(t)$

$$\left\{ \begin{array}{l} \frac{\partial n(v,t)}{\partial t} + \frac{\partial}{\partial v} [(-v + bN(t))n(v,t)] - a(N(t)) \frac{\partial^2 n(v,t)}{\partial v^2} = \frac{R(t)}{\tau} \delta_{V_R}(v), \\ n(V_F, t) = 0, \quad n(-\infty, t) = 0 \\ N(t) := -a(N(t)) \frac{\partial}{\partial v} n(V_F, t) \geq 0 \\ \frac{d}{dt} R(t) + \frac{R(t)}{\tau} = N(t). \quad \text{Refractory state} \end{array} \right.$$

(See also Brunel for other versions)

## Theorem (M.Cáceres, BP) [Refractory]

The solution blows-up in finite time in the 2 cases :

- $b > 0$  is fixed, if the initial data is concentrated enough around  $V_F$ .
- The initial data is given, if  $b$  large enough

**Proof.** For  $\mu = 2 \max(\frac{1}{b}, \frac{V_F}{a_0})$ , define

$$\phi(v) = e^{\mu v}, \quad M_\mu(t) := \int_{-\infty}^{V_F} \phi(v) n(v, t).$$

For smooth solutions, we prove that  $M_\mu(t)$  becomes larger than  $e^{\mu V_F}$

$$\begin{aligned} \frac{dM_\mu}{dt} &= \mu \int_{-\infty}^{V_F} (bN(t) - v + \mu a) \phi(v) p(v, t) - N(t) \phi(V_F) + \frac{R(t)}{\tau} \phi(V_R) \\ &\geq N(t) \underbrace{[b\mu M_\mu(t) - \phi(V_F)]}_{\substack{\geq \mu V_F > 0 \\ > 0 \text{ is needed only initially}}} + \underbrace{\mu[\mu a_0 - V_F]}_{\geq \mu V_F > 0} M_\mu(t) \end{aligned}$$

OK for  $b$  large enough or  $M_\mu(0)$  large enough

To go further : the difficulty : no relation between  $M_\mu$  and  $N$

**Open question** : coupling an inhibitory and excitatory network.

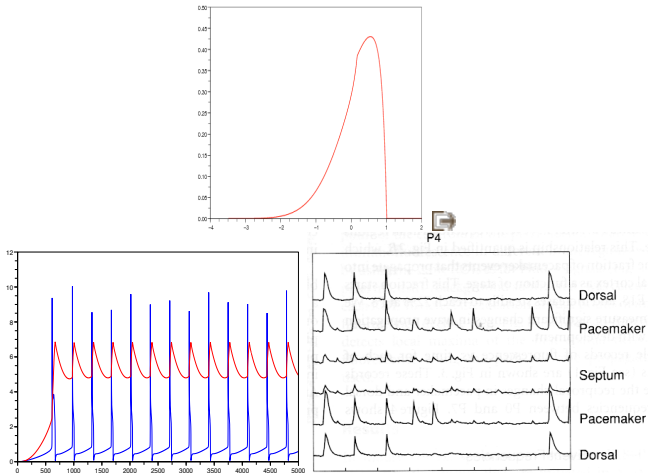
Assume refractory state and that the firing potential  $V_F$  is random.

$$\begin{aligned} \frac{\partial n(v,t)}{\partial t} + \frac{\partial}{\partial v} [(-v + bN(t))n(v,t)] - a(N(t)) \frac{\partial^2 n(v,t)}{\partial v^2} + \frac{n(v,t)}{\varepsilon} \mathbb{1}_{\{v > V_F\}} \\ = \frac{R(t)}{\tau} \delta_{V_R}(v), \end{aligned}$$

$$\left\{ \begin{array}{l} N(t) := - \int \frac{n(v,t)}{\varepsilon} \mathbb{1}_{\{v > V_F\}} dv \\ \frac{d}{dt} R(t) + \frac{R(t)}{\tau} = N(t). \end{array} \right. \quad \text{Refractory state}$$

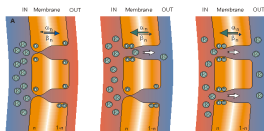
Solutions are globally bounded.

# Spontaneous activity (regularized)



Left : Excitatory integrate and fire model with refractory state and random firing threshold

Right : Conhaim et al (2011) J. of physiology 589(10) 2529-2541.



From J. Malmivuo and R. Plonsey, Principles and Appl. of bioelectric and biomagnetic fields, OUP 1995

Ion channels lead to ODE models *à la* Hodgkin-Huxley

$$\frac{\partial}{\partial t} p(v, g, t) + \frac{\partial}{\partial v} [(-g_L v + g(V_E - v)) p(v, g, t)]$$

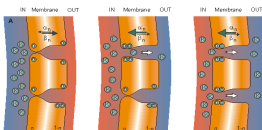
$$+ \frac{\partial}{\partial g} \left[ \frac{N(t) - g}{\sigma_E} p(v, g, t) \right] - \frac{a(t)}{\sigma_E} \frac{\partial^2}{\partial g^2} p(v, g, t) = 0,$$

$$v \in (0, V_F), \quad g \geq 0,$$

Cai, Shelley, McLaughlin, Rangan, Kovacic, Ly, Trnachina...

Sub-elliptic fluxes





From J. Malmivuo and R. Plonsey, Principles and Appl. of bioelectric and biomagnetic fields, OUP 1995

Ion channels lead to ODE models *à la* Hodgkin-Huxley

$$\frac{\partial}{\partial t} p(v, g, t) + \frac{\partial}{\partial v} [(-g_L v + g(V_E - v)) p(v, g, t)] + \frac{\partial}{\partial g} \left[ \frac{N(t) - g}{\sigma_E} p(v, g, t) \right] - \frac{a(t)}{\sigma_E} \frac{\partial^2}{\partial g^2} p(v, g, t) = 0,$$

$$v \in (0, V_F), \quad g \geq 0,$$

## Theorem (D. Salort, BP)

- Stationary solutions belong to  $L^{\frac{8}{7}-}$
- Evolution solutions are globally bounded in  $L^p$  (no blow-up)



Based on K. Pakdaman, J. Champagnat, J.-F. Vibert

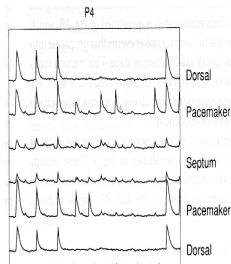
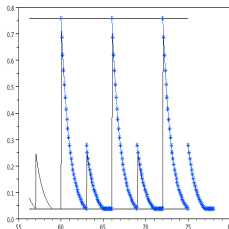
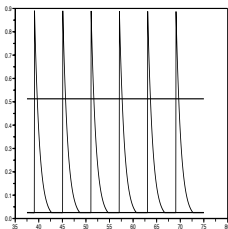
- $s$  represents the time elapsed since the last discharge
- $n(s, t)$  probability of finding a neuron in 'state'  $s$  at time  $t$
- $N(t) =$  activity of the network

$$\frac{\partial n(s, t)}{\partial t} + \overbrace{\frac{\partial n(s, t)}{\partial s}}^{\text{elapsed time advances}} + \overbrace{r(s, bN(t)) n(s, t)}^{\text{firing neurons}} = 0,$$

$$N(t) := n(s = 0, t) = \underbrace{\int_0^{+\infty} r(s, bN(t)) n(s, t) ds}_{\text{neurons reset}}$$

$$\frac{\partial n(s,t)}{\partial t} + \overbrace{\frac{\partial n(s,t)}{\partial s}}^{\text{elapsed time advances}} + \overbrace{r(s, bN(t)) n(s,t)}^{\text{firing neurons}} = 0,$$

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Right : Conhaim et al (2011) J. of physiology 589(10) 2529-2541.

- For the Noisy LIF model synchronization arises as a singularity of the total activity of the network

- But there are regimem with smooth solutions and total desynchronization

- Open problems ■ coupled inhibitory/excitatory

- convergence to a steady state (inhibitory)

- Derivation of LIF models

## THANKS TO MY COLLABORATORS

M. J. Carceres, J. A. Carrillo

D. Smets, D. Salort

K. Pakdaman

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K. Pakdaman

# THANK YOU